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(54) **FLUID EJECTION DEVICE AND MEDICAL INSTRUMENT**

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See application file for complete search history.

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Related U.S. Application Data

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(57) **ABSTRACT**

(51) **Int. Cl.**

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A fluid ejection device includes a pulsation generator which converts a fluid into a pulsed fluid, a fluid supply unit (supply pump) which supplies the fluid to the pulsation generator, an ejection tube which has an ejection opening communicating with the pulsation generator, a suction tube into which the ejection tube is inserted with play, a suction channel provided between the suction tube and the ejection tube, a suction opening provided at an end of the suction channel in a vicinity of the ejection opening, and a suction unit (suction pump) which sucks fluid in such a manner that the fluid introduced from the suction opening passes through the suction channel. The ejection opening is held by an inner circumferential part of the suction opening. According to this structure, vibration of the ejection tube in the vicinity of the ejection opening can be reduced.

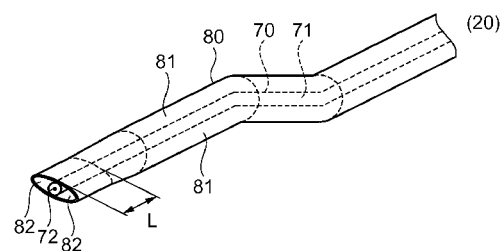
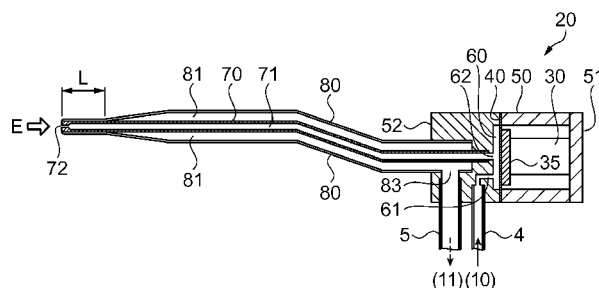
(52) **U.S. Cl.**

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5 Claims, 4 Drawing Sheets



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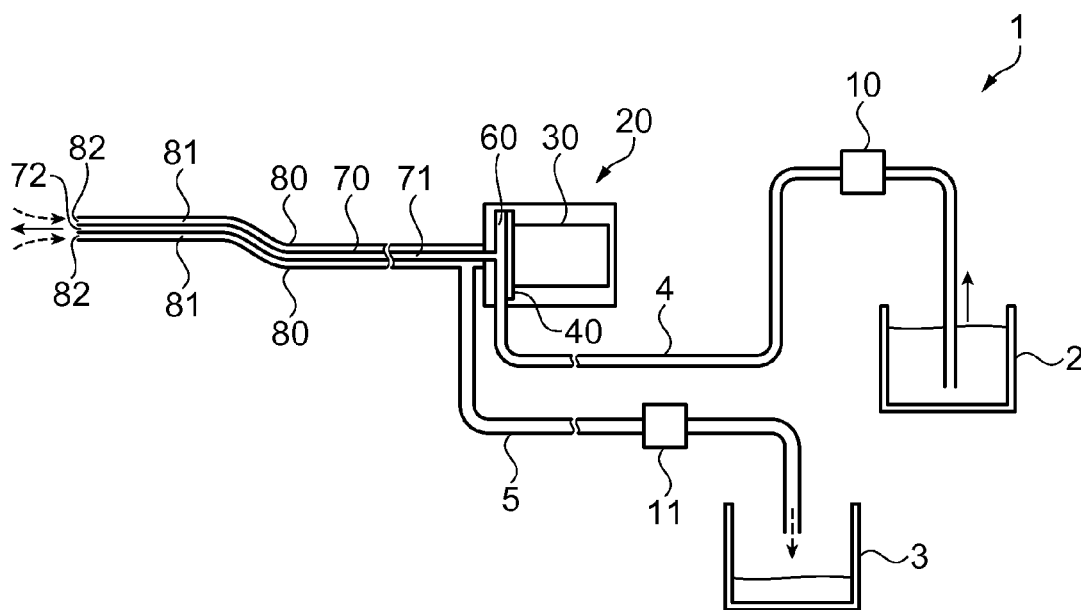


FIG. 1

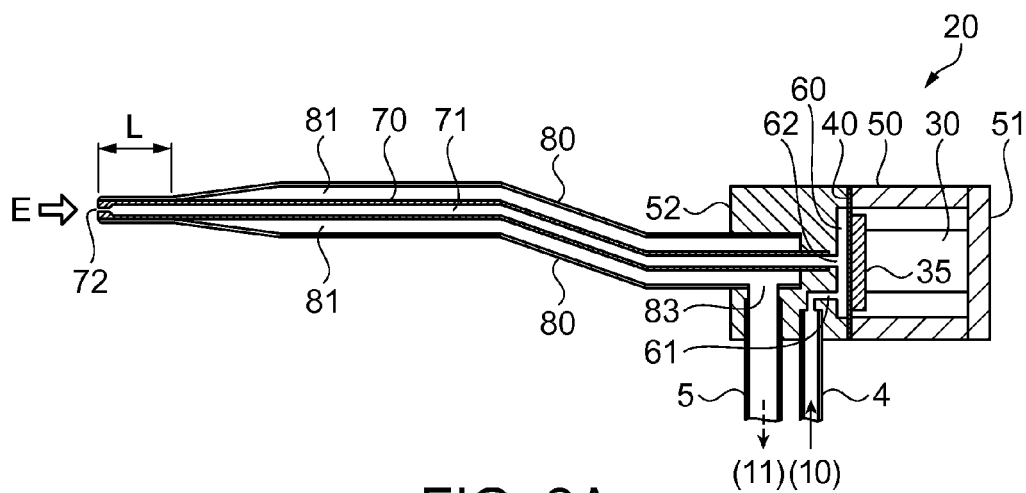


FIG. 2A

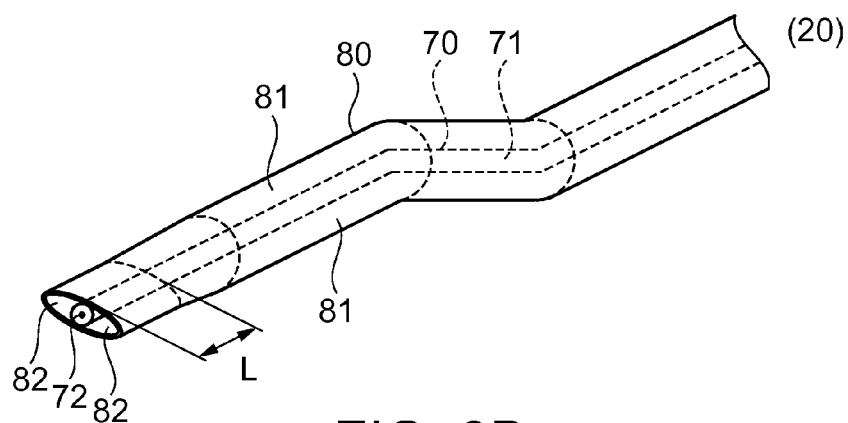


FIG. 2B

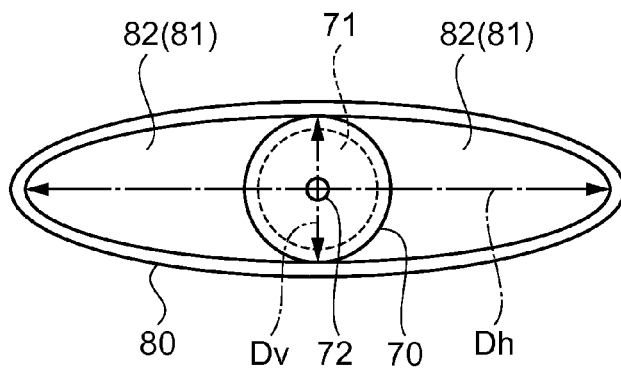


FIG. 2C

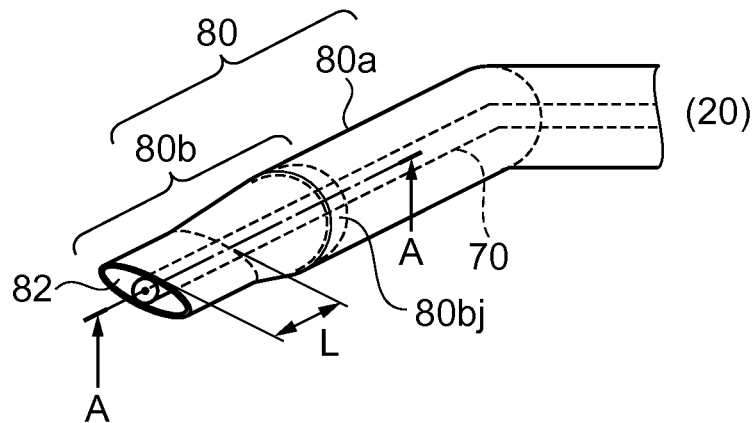


FIG. 3A

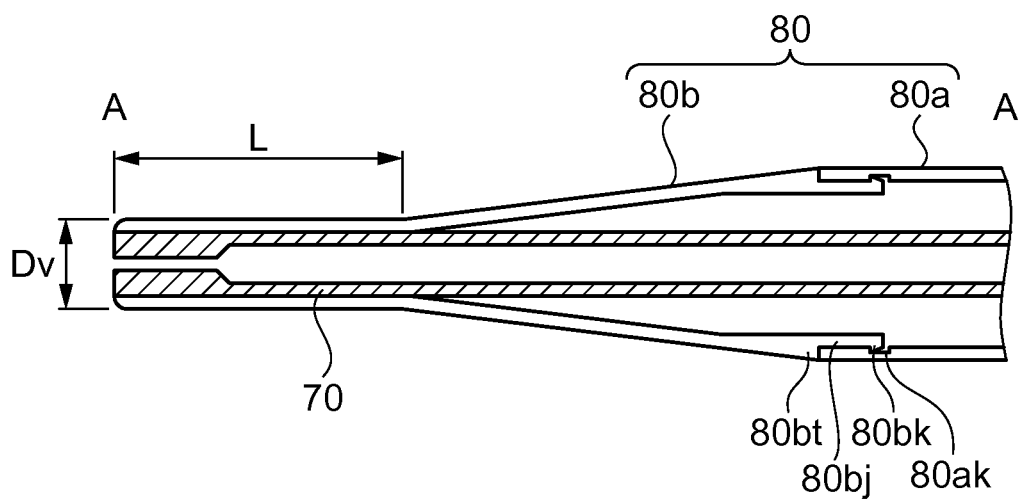


FIG. 3B

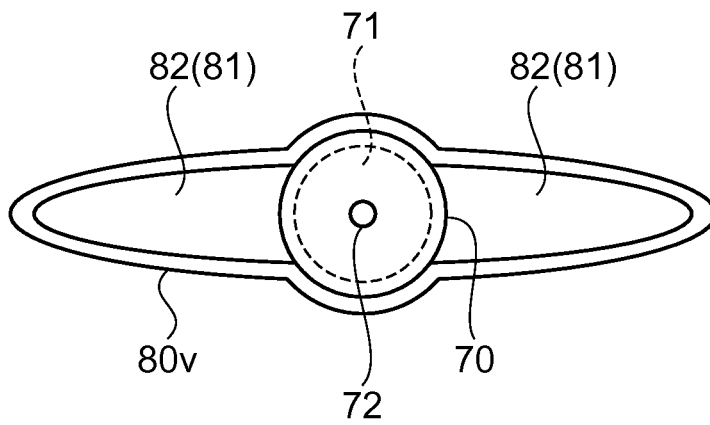


FIG. 4A

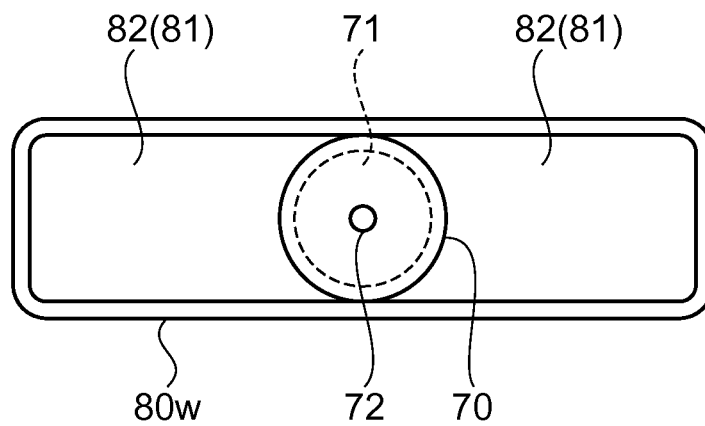


FIG. 4B

FLUID EJECTION DEVICE AND MEDICAL INSTRUMENT

CROSS-REFERENCE TO RELATED APPLICATIONS

The present application is a Continuation of U.S. patent application Ser. No. 13/269,885, filed on Oct. 10, 2011, which claims priority to Japanese Patent Application No: 2010-229325, filed Oct. 12, 2010, which applications are expressly incorporated by reference herein.

BACKGROUND

1. Technical Field

Embodiments of the present invention relate to a fluid ejection device, and a medical instrument including the fluid ejection device.

2. Related Art

A fluid ejection device capable of excising, incising, and crushing living tissue has excellent characteristics when used as a surgical instrument. A low probability of heat damage and preservation of blood vessels including capillaries are examples of these characteristics.

During surgery, a surgery target may become obscured from view while using the fluid ejection device. A certain type of fluid ejection device has a suction tube which sucks and removes the ejected liquid, excised tissue or the like remaining on the surgery target so as to ensure that the surgery target remains visible during surgery.

This type of fluid ejection device includes an ejection tube through which high-pressure fluid is ejected. The ejection tube is disposed within a suction channel of a suction tube in such a position so as to be concentric with the suction channel (for example, see JP-A-1-313047).

Another example of the fluid ejection device has an ejection tube through which high-pressure fluid is ejected. This ejection tube is inserted into a suction tube eccentrically with respect to the inner circumferential surface of the suction tube (for example, see JP-A-6-90957).

A further example of the fluid ejection device is equipped with a volume varying unit which rapidly varies the volume of a fluid chamber so as to convert the fluid into a pulsed fluid. The fluid is thus ejected in pulses at high speed through an ejection opening (for example, see JP-A-2008-82202).

According to the fluid ejection devices disclosed in JP-A-1-313047 and JP-A-6-90957, however, the ejection tube vibrates when fluid is ejected in pulses at high speed when using the technology disclosed in JP-A-2008-82202. More specifically, the ejection tube provided within the suction tube is not supported or fixed except at the root of the ejection tube. As a result, vibrations occur at the tip of the ejection tube when fluid is ejected in pulses at high speed. Several problems arise from the vibrations that occur at the tip of the ejection tube. For example, there is a decrease in the positional accuracy of the fluid ejection. In addition, vibration noise is generated by the interference between the ejection tube and the suction tube into which the ejection tube is inserted.

To overcome these problems, a structure has been adopted which includes a support member within the suction tube to firmly support the ejection tube. However, this structure is complicated. In addition, this structure deteriorates the maneuverability of the fluid ejection device due to the increased size and weight of the fluid ejection device resulting from this structure.

SUMMARY

An advantage of some aspects of embodiments the invention is to solve at least a part of the aforementioned problems. Embodiments of the invention can be implemented according to the following forms or application examples.

Application Example 1

This application example is directed to a fluid ejection device including: a pulsation generator which converts fluid into a pulsed fluid; a fluid supply unit which supplies the fluid to the pulsation generator; an ejection tube which has an ejection opening communicating with the pulsation generator; a suction tube into which the ejection tube is inserted with play; a suction channel provided between the inner circumferential surface of the suction tube and the outer circumferential surface of the ejection tube; a suction opening provided at the end of the suction channel in the vicinity of the ejection opening; and a suction unit which sucks the fluid in such a manner that the fluid introduced from the suction opening passes through the suction channel. The ejection opening is held by an inner circumferential part of the suction opening.

According to this application example of the invention, the ejection opening of the ejection tube is held by the inner circumferential part of the suction tube. In this case, the tip of the ejection tube does not easily vibrate during high-speed ejection of pulsed fluid. In the case of the fluid ejection device which has the ejection tube inserted into the suction tube with play provided therebetween (e.g., between the ejection tube and the suction tube), both an increase in the positional accuracy of the fluid ejection and a reduction of abnormal noise can be achieved by a simple structure without increasing the size and weight of the fluid ejection device.

Application Example 2

This application example of the invention is directed to the fluid ejection device of the above application example. In this application example, across-sectional shape of the suction opening in the direction perpendicular to the extending direction of the suction tube is a flat shape.

According to this application example of the invention, the cross-sectional shape of the suction opening has a flat shape or a flattened shape. In one example, the cross-sectional shape of the suction opening or the tip of the suction tube may be flatter than another portion of the suction tube. In this case, the suction opening can be sufficiently opened under the condition in which the ejection tube is held by the inner circumferential surface of the suction tube. The flat shape of the suction opening, for example, may be expanded upon insertion of the ejection tube, which sufficiently opens the suction opening for sucking. Moreover, the suction tube having the flat portion in the vicinity of the suction opening (tip portion of the ejection tube) can be easily inserted into a narrow surgery target portion, which further improves the maneuverability of the fluid ejection device.

Application Example 3

This application example of the invention is directed to the fluid ejection device of the above application example. In this application example, across-sectional shape of the

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suction opening in the direction perpendicular to the extending direction of the suction tube is a substantially elliptic shape.

According to this application example of the invention, the cross-sectional shape of the suction opening has a substantially elliptic shape. In this case, a sufficient opening area of the suction opening can be produced. The portion corresponding to the major axis of the elliptic shape of the suction opening under the condition in which the ejection tube is held by the portion of the suction opening corresponding to the minor axis of the elliptic shape of the suction opening provides the opening area. Moreover, the suction tube having a flat shape formed by the elliptic shape in the vicinity of the suction opening can be easily inserted into a narrow surgery target portion, which further improves the maneuverability of the fluid ejection device. Furthermore, the suction opening having the substantially elliptic shape is not easily caught by the surgery target portion. Even when the suction opening contacts the surgery target portion, the surgery target portion is not damaged thereby.

Application Example 4

This application example of the invention is directed to the fluid ejection device of the above application example. In this application example, the ejection opening is positioned substantially at a center of the suction opening.

According to this application example of the invention, the ejection opening is positioned substantially at the center of the major axis of the suction tube. Thus, the position of the ejection opening is easily recognized, which facilitates ejection of the fluid toward the surgery target portion.

Application Example 5

This application example of the invention is directed to the fluid ejection device of the above application example. In this application example, the tip of the suction tube including the suction opening engages with the suction tube in such a manner so as to be rotatable around the axis of the suction tube.

According to this application example of the invention, the tip of the suction tube is rotatable around the axis of the suction tube. In this case, the direction of the tip of the suction tube can be controlled in accordance with the shape of the surgery target portion. Thus, the maneuverability of the fluid ejection device further improves.

Application Example 6

This application example of the invention is directed to a medical instrument including the fluid ejection device of the above application example of the invention.

A medical instrument including the fluid ejection device of the above application example of the invention can effectively provide excellent characteristics of a surgery instrument.

BRIEF DESCRIPTION OF THE DRAWINGS

Embodiments of the invention will be described with reference to the accompanying drawings, wherein like numbers reference like elements.

FIG. 1 illustrates a structure of a fluid ejection device according to a first embodiment.

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FIG. 2A is a side cross-sectional view showing example structures of a pulsation generator, an ejection tube, and a suction tube according to a first example.

FIG. 2B is a perspective view showing an example of the tip structure of the ejection tube and the suction tube.

FIG. 2C is a front view showing examples of the tips of the ejection tube and the suction tube as viewed from the tip side (E direction in FIG. 2A).

FIG. 3A is a perspective view showing an example of a tip structure of an ejection tube and a suction tube according to a second example.

FIG. 3B is a cross-sectional view taken along a line A-A in FIG. 3A.

FIG. 4A is a front view showing examples of tips of an ejection tube and a suction tube as viewed from the tip side according to a third example.

FIG. 4B is a front view showing examples of tips of an ejection tube and a suction tube as viewed from the tip side according to a fourth example.

DESCRIPTION OF EXEMPLARY EMBODIMENT

Embodiments according to the invention are hereinafter described with reference to the drawings. Scales different from the actual ones are set for components and parts shown in the respective figures so that these components and parts can be expanded to sufficient sizes easily recognizable in the figures.

First Embodiment

FIG. 1 illustrates a structure of a fluid ejection device according to a first embodiment. In this embodiment, a fluid ejection device included in a medical instrument will be discussed. The fluid ejection device in this embodiment includes, but is not limited to, functions such as excision, incision, exfoliation, and crushing. Further, the fluid ejection device is not limited to applications in the medical field.

As illustrated in FIG. 1, a fluid ejection device 1 includes a fluid supply container 2 storing fluid, a supply pump 10 as a fluid supply unit, a pulsation generator 20 which converts fluid supplied from the supply pump 10 into pulsed fluid, an ejection tube 70 which communicates with the pulsation generator 20, a suction tube 80 which extends from the pulsation generator 20, a suction pump 11 as a suction unit, and a waste fluid container 3 which stores sucked waste liquid and excised tissue. The pulsation generator 20, the supply pump 10, and the fluid supply container 2 are connected with one another via a fluid supply channel tube 4. The suction tube 80, the suction pump 11, and the waste fluid container 3 are connected with one another via a suction channel tube 5.

The pulsation generator 20 may be constituted by any type of generator that can eject fluid in pulses. Examples include a piezoelectric type and a bubble jet type. In this embodiment, the pulsation generator 20 includes a piezoelectric type generator. Fluid used herein may be physiological salt water as an example, although other fluids are within the scope of the disclosure. The ejection tube 70 includes an ejection channel 71 communicating with a fluid chamber 60 formed within the pulsation generator 20, and an ejection opening 72 disposed at a tip of the ejection tube 70. The ejection opening 72 may be configured as an opening having a reduced flow channel width.

The ejection tube 70 is inserted into the suction tube 80 with play provided therebetween. The ejection tube 70 may

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be held by a part of the inner circumferential surface of the suction tube **80** in the vicinity of the ejection opening **72**. The space formed between the inner circumferential surface of the suction tube **80** and the outer circumferential surface of the ejection tube **70** corresponds to or defines a suction channel **81**. A suction opening **82** is provided at the end of the suction channel **81** in the vicinity of the ejection opening **72**. In one example, the ejection tube **70** is rigid enough to not be deformed by fluid pressure produced at the time of fluid ejection. The suction tube **80** is rigid enough to not be deformed by negative pressure produced by the suction pump **11**.

The flow of fluid produced by the fluid ejection device **1** as constructed is now briefly explained. Fluid stored in the fluid supply container **2** is sucked by the supply pump **10**, and supplied to the pulsation generator **20** via the fluid supply channel tube **4** at constant pressure in one embodiment.

The pulsation generator **20** includes the fluid chamber **60**, a piezoelectric device **30** as a volume varying unit which varies the volume of the fluid chamber **60**, and a diaphragm **40**. The pulsation generator **20** actuates the piezoelectric device **30** to generate a pulsed flow within the fluid chamber **60**. This pulsed flow passes through the ejection channel **71**, and comes out of the ejection opening **72** as a high-speed ejection flow in pulses.

When the pulsation generator **20** stops operation, that is, does not change the volume of the fluid chamber **60**, the fluid supplied from the supply pump **10** at constant pressure passes through the fluid chamber **60** and comes out of the ejection opening **72** as a continuous ejection flow.

The pulsed flow of fluid herein refers to a flow of fluid whose flow direction is kept constant or substantially constant and whose flow amount or flow speed changes periodically or irregularly. The pulsed flow includes an intermittent flow that repeatedly flows and stops. However, the pulsed flow may include other types of flow as long as the flow amount or flow speed of fluid changes periodically or irregularly.

Similarly, the ejection of fluid in pulses refers to the ejection of fluid whose flow amount or moving speed varies periodically or irregularly. The ejection of fluid in pulses includes an intermittent ejection which repeats the ejection and non-ejection of fluid, for example. However, the ejection in pulses may include other types of ejection as long as the flow amount or moving speed of fluid to be ejected changes periodically or irregularly.

The suction mechanism is now explained. The fluid ejected from the ejection opening **72** remains on the surgery target portion as waste liquid. Moreover, excised living tissue (hereinafter abbreviated as excised tissue) stays on the surgery target portion as well. The waste liquid and excised tissue are sucked by the suction pump **11** through the suction opening **82**, and passed through the suction channel **81** and the suction channel tube **5** to be stored in the waste fluid container **3**. The operation of the suction pump **11** may be initiated in correlation with the operation of the pulsation generator **20**. Alternatively, the suction pump **11** may be intermittently operated at regular intervals, or only operated as necessary.

There are several shapes and structures of the ejection tube **70** and the suction tube **80** considered as appropriate examples. The details of these shapes and structures are hereinafter described as specific examples in conjunction with the associated drawings.

First Example

FIG. **2A** is a side cross-sectional view of the pulsation generator, the ejection tube, and the suction tube according

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to the first example taken along a plane extending in the flow direction of the fluid. FIG. **2B** is a perspective view illustrating a tip structure of the ejection tube and the suction tube. FIG. **2C** is a front view illustrating example tips of the ejection tube and the suction tube as viewed from the tip direction (direction of E in FIG. **2A**).

As illustrated in FIG. **2A**, the pulsation generator **20** includes an inlet channel **61** through which fluid supplied from the supply pump **10** via the fluid supply channel tube **4** is introduced into the fluid chamber **60**. The pulsation generator **20** also includes the piezoelectric device **30** and the diaphragm **40** as the volume varying unit for varying the volume of the fluid chamber **60**, and an outlet channel **62** communicating with the fluid chamber **60**.

The diaphragm **40** is formed by a disk-shaped metal thin plate in this example, and is fixed by close contact with a lower case **50** and an upper case **52**. The piezoelectric device **30** is a laminated piezoelectric device in this example. One of the ends of the piezoelectric device **30** is fixed to the diaphragm **40** via an upper plate **35**, while the other end of the piezoelectric device **30** is fixed to a bottom plate **51**.

The liquid chamber **60** is a space produced between the diaphragm **40** and a recess formed on the surface of the upper case **52** opposed to the diaphragm **40**. The outlet channel **62** is opened substantially at the center of the fluid chamber **60** in this example.

The upper case **52** and the lower case **50** are joined to each other via the opposed faces thereof to be formed into one body (in the example shown in FIG. **2A**, the diaphragm **40** is interposed between the cases **52** and **50**). The ejection tube **70** may be inserted into the upper case **52** by press-fit. The ejection tube **70** includes the ejection channel **71** which communicates with the outlet channel **62**. The ejection opening **72** may have a reduced channel diameter and is opened at the tip of the ejection tube **70**. The ejection opening **72** may be provided as a nozzle.

The suction tube **80** provided as a jacket tube of the ejection tube **70** extends from the upper case **52**. An opening **83** is formed in the vicinity of the root end of the suction tube **80** on the side close to the pulsation generator **20** in such a manner as to penetrate the tube wall of the suction tube **80**. The suction channel tube **5** attached to the opening **83** communicates with the opening **83**.

According to this structure, the extending direction of the suction channel tube **5** in the vicinity of the pulsation generator **20** is equalized with the direction of the fluid supply channel tube **4**. In this case, the maneuverability of the fluid ejection device **1** improves when the ejection device **1** is used by an operator (operator of the ejection device) who holds the pulsation generator **20** during operation of the fluid ejection device **1**. The ejection tube **70** and the suction tube **80** may be tubes extending in straight lines. However, the tubes **70** and **80** may be bent as illustrated in FIG. **2A** so that visibility around the ejection opening **72** can be secured without the hand and fingers of the operator holding the fluid ejection device **1** impeding visibility around the ejection opening **72**.

As illustrated in FIGS. **2B** and **2C**, the tip of the ejection tube **70** in the vicinity of the ejection opening **72** is held by a flat part of the inner circumferential surface of the suction tube **80**. More specifically, the cross section of a holding area L of the suction tube **80** in the vicinity of the suction opening **82** has a substantially elliptic shape having a major axis Dh and a minor axis Dv such that two points of the ejection tube **70** opposed to each other approximately in the direction of the diameter can be held by the part of the suction tube **80** corresponding to the position of the minor axis Dv.

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While the suction tube **80** has a flat shape produced by the substantially elliptic cross section in this example, the direction of flatness is not limited to this direction. For example, the suction tube **80** may have a substantially elliptic shape which has the major axis D_v and the minor axis D_h . In addition, while only the tip portion of the suction tube **80** has the substantially elliptic shape in this example, the entire shape as well as the tip portion of the suction tube **80** may be substantially elliptic when at least the part of the ejection tube in the vicinity of the ejection opening is held by the inner circumferential part of the suction tube.

The suction channel **81** and the suction opening **82** are formed by the space between the outer circumference of the ejection tube **70** and the inner circumference of the suction tube **80**. In this case, as illustrated in FIGS. 2B and 2C, the space corresponding to the suction channel **81** and the suction opening **82** in the holding area L becomes wider as the major axis D_h of the substantially elliptic cylindrical shape of the suction tube **80** increases. When the two points of the ejection tube **70** opposed to each other approximately in the direction of the diameter are held by the part of the suction tube **80** corresponding to the position of the minor axis D_v , substantially the same opening area is produced in the suction opening **82** on each side of the ejection opening **72**. In other words, the ejection opening **72** is positioned substantially at the center of the major axis D_h in one example.

The ejection tube **70** can be fixed to the suction tube **80** by applying an adhesive, a solder or other fixing materials to the portion of the inner circumference of the suction tube **80** holding the outer circumference of the ejection tube **70**. Alternatively, the ejection tube **70** may be held and fixed by pressing and deforming the portion of the suction tube **80** corresponding to the holding area L such that this portion becomes a flat portion after the ejection tube **70** is inserted into the suction tube **80** with play provided between the ejection tube **70** and the suction tube **80**. The length of the holding area L may be arbitrarily determined as long as the ejection tube **70** can be securely held and fixed by the length of the holding area L. Thus, the holding area L may be provided only at the tip of the ejection tube **70**.

According to the fluid ejection device in this example, the following advantages can be offered.

The area of the ejection tube **70** in the vicinity of the ejection opening **72** can be easily held and fixed without using an additional support member provided within the suction tube **80**. According to this structure, at least two points of the ejection tube **70** opposed to each other in the direction of the diameter can be held by the suction tube **80**, in which condition the ejection tube **70** can be more firmly fixed.

Since the area of the ejection tube **70** around the ejection opening **72** is held by the suction tube **80** in one example, vibration at the tip of the ejection tube **70** can be reduced during a high-speed ejection of a pulsed flow. Thus, even in the case of the fluid ejection device having the structure in which the ejection tube **70** is inserted into the suction tube **80** with play provided therebetween, a high-speed ejection of fluid in pulses toward the surgery target position can be accurately achieved. Moreover, in the condition where the outer circumference of the ejection tube **70** is directly held by the inner circumference of the suction tube **80**, abnormal noise, which might be generated due to vibration by the contact between the ejection tube **70** and the suction tube **80**, is not generated.

The cross section of the portion of the suction tube **80** corresponding to the holding area L has a substantially

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elliptic shape in one example. Thus, when the major axis D_h of the suction tube **80** is long, the suction tube **80** obtains a sufficient opening area of the suction opening **82** while holding and fixing the ejection tube **70**. In other words, the suction opening **82** of the suction tube **80** is sufficiently open to enable suction.

The portion of the suction tube **80** in the holding area L has the flat shape corresponding to the elliptic cross-sectional shape. In this case, the fluid ejection device **1** can be easily inserted into a narrow surgery target portion such as an incision target and an exfoliation target. Thus, the maneuverability of the fluid ejection device **1** during surgery is further improved.

The ejection opening **72** is disposed substantially at the center of the major axis D_h of the suction tube **80**. Accordingly, the operator can easily recognize the position of the ejection opening **72** and can easily operate the fluid ejection device **1** to eject fluid toward the surgery target.

According to this example, therefore, vibration of the ejection tube **70** and abnormal noise generated thereby can be reduced by a simple structure without increasing the size and weight of the fluid ejection device **1**. Further, fluid can be accurately ejected from the fluid ejection device **1** toward an accurate target position. The maneuverability of the fluid ejection device **1** is improved.

Second Example

A second example is now described with reference to the drawings. FIG. 3A is a perspective view illustrating an example of a tip structure of the ejection tube and the suction tube according to the second example. FIG. 3B is a cross-sectional view taken along a line A-A in FIG. 3A. According to the first example, the suction tube **80** is constituted by a single piece structure. In this example, however, the tip portion of the suction tube **80** is a component that can be separated from the suction tube **80** and that engages with the suction tube **80** in such a manner as to be rotatable around the axis of the suction tube **80**. Components and parts in this example which correspond to similar components and parts in the first example have been given similar reference numbers, and the same explanation is not repeated.

As illustrated in FIG. 3A, the suction tube **80** has a tip portion **80b**, and a suction tube portion **80a** extending between the pulsation generator **20** and the tip portion **80b**. The tip portion **80b** engages with the suction tube portion **80a**.

The tip portion **80b** includes the area corresponding to the holding area L, and a joint **80bj** which can be inserted into the suction tube **80a** for engagement therewith and sliding thereon in such a manner as to be rotatable. The tip portion **80b** also includes an engaging portion provided between the holding area L and the joint **80bj**. In the engaging portion, the minor axis D_v of the substantially elliptic cylinder gradually increases to produce a substantially circular shape.

The joint **80bj** is a cylindrical component constituting an engaging portion between the tip portion **80b** and the suction tube portion **80a**. The joint **80bj** extends from the end of the tip portion **80b** on the side contacting the suction tube portion **80a**. The outer circumference of the joint **80bj** contacts the inner circumference of the engaging area of the suction tube portion **80a** and slides thereon in such a manner as to be rotatable. The tip portion **80b** can be rotated with respect to the suction tube portion **80a**. Stoppers **80bt** and **80bk** are provided on the extended portion of the joint **80bj**. The stopper **80bt** is a part for preventing the tip portion **80b** from being excessively inserted into the suction tube portion

80a by the negative pressure produced by the suction pump **11**. The stopper **80bk** is a part for preventing separation of the tip portion **80b** from the engagement with the suction tube portion **80a**. A notch **80ak** corresponding to the shape of the stopper **80bk** is provided on the suction tube portion **80a**. When the tip portion **80b** is inserted in the suction tube portion **80a**, the notch **80ak** engages with the stopper **80bk**.

The outer circumference of the joint **80bj** slides on the inner circumference of the suction tube portion **80a**, and the area of the outer circumference of the ejection tube **70** corresponding to the holding area **L** slides on the inner circumference of the tip portion **80b**. As a result, the tip portion **80b** can rotate with respect to the suction tube portion **80a** around the axis thereof. According to the first example, a fixing material such as an adhesive and a solder is applied to the portion where the outer circumference of the ejection tube **70** is held by the inner circumference of the suction tube **80**. In this example, however, such a fixing material is not applied to this area to allow sliding and/or rotation of the tubes **70** and **80** relative to each other. The tip portion **80b** can slide in at least a rotational motion. The fluid ejection device in this example can provide at least the following advantages. According to this structure, the tip portion **80b** is rotatable with respect to the suction tube portion **80a** around the axis thereof.

In one example, the operator can control the direction of the suction opening in accordance with the shape of the surgery target portion. More specifically, the direction of the tip portion **80b** having a flat shape can be varied (e.g., by rotating the tip portion **80b**) according to the shape of a narrow surgery target portion such as an incision target, or changed in such a direction that the surgery target portion can be easily seen.

Accordingly, the fluid ejection device in this example can offer an advantage of further improvement over the maneuverability of the fluid ejection device as well as the advantages provided in the first example.

Third Example

A third example is now described with reference to the drawings. FIG. 4A is a front view of example tips of the ejection tube and the suction tube according to the third example as viewed from the tip side (direction of **E** in FIG. 2A). According to the first and second examples, the suction tube **80** has a substantially elliptic cross section in the holding area **L** (FIG. 2C). However, the cross section in each of the tips may have a shape of a suction tube **80v** shown in FIG. 4A. Components and parts in this example which correspond to similar components and parts in the above examples have been given similar reference numbers, and the same explanation is not repeated.

The suction tube **80v** has a flat shape produced by further pressing the suction tube **80** having the substantially elliptic shape in the first and second examples against the ejection tube **70**. The suction tube **80v** holds the ejection tube **70** via the surface of the suction tube **80v** extending almost along the curvature of the outer circumference of the ejection tube **70**. In this example, approximately half the area of the outer circumferential surface of the ejection tube **70** in the holding portion (holding area **L**) is held by the inner circumference of the suction tube **80v**.

According to this example, therefore, the suction tube **80v** can more firmly hold the ejection tube **70**. The suction tube **80v** is pressed flat to shape a portion of the suction tube **80v** against more of the outer circumferential surface of the ejection tube **70** than previous examples. The suction tube

80v thus follows the shape of the ejection tube **70**. Moreover, the suction tube **80v** has a more flat shape and can be easily inserted into a narrower surgery target portion such as an incision target or an exfoliation target, which improves the maneuverability of the fluid ejection device during surgery.

Fourth Example

A fourth example is now described with reference to the drawings. FIG. 4B is a front view of example tips of the ejection tube and the suction tube according to the fourth example as viewed from the tip side. The cross-sectional shape of the suction tube **80** in the holding area **L** according to each of the first and second examples may have a shape of a suction tube **80w** shown in FIG. 4B. Components and parts in this example which correspond to similar components and parts in the above examples have been given similar reference numbers, and the same explanation is not repeated.

The tip of the ejection tube **70** in the vicinity of the ejection opening **72** is held by the inner circumference of the suction tube **80w** having a flat shape. More specifically, the cross section of the suction tube **80w** in the holding area **L** has a substantially rectangular shape in this example. The length of the short side of the rectangular shape is substantially equivalent to the outside diameter of the ejection tube **70** being held. The centers of the two long sides of the suction tube **80w** substantially hold two points of the ejection tube **70** opposed to each other in the direction of the diameter. Each of the four corners of the cross section of the substantially rectangular shape has a round shape for protecting the surgery target in contact with the suction tube **80w** in one example.

According to this example, the width of the suction tube **80w** in the vicinity of the suction opening **82** is equivalent to each of the corresponding widths of the suction tube **80** (FIG. 2C) and the suction tube **80v** (FIG. 4A). However, the opening area of the suction opening **82** becomes wider due to the rectangular cross section. Thus, the fluid and the excised tissue can be further efficiently sucked and removed through the suction tube.

Medical Instrument

A medical instrument including the fluid ejection device **1** described herein can more effectively provide excellent characteristics of a surgery instrument. More specifically, the fluid ejection device **1** has excellent characteristics as a surgery instrument including low probabilities of heat damage and preservation of blood vessels including capillaries at the time of excision, incision, crush and the like of living tissue. Both the pulsed flow ejection which allows execution of surgery by using a small amount of physiological salt water, and the provision of the suction tube **80** around the ejection tube **70** can help prevent the fluid and excised tissue from blocking the vision of an operator of the fluid ejection device, thereby securing visibility for surgery. The position of the ejection tube **70** substantially at the center of the suction tube **80** allows the operator to easily recognize the position of the ejection opening **72** and allows the operator to easily eject fluid toward the surgery target accurately. The tip portion of the ejection opening **72** under the held and fixed condition does not vibrate during high-speed fluid ejection in pulses, which permits the high-speed pulsed fluid ejection to be directed toward the position of the surgery target with accuracy. Moreover, elimination of abnormal noise generated with vibration allows the operator to concentrate his or her attention further on the surgery.

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What is claimed is:

1. A medical instrument comprising:

a pulsation generator for converting a fluid into a pulsed fluid including;

a fluid chamber accommodating the fluid; and

a pressure generator for applying pressure to a fluid within the fluid chamber and converting the fluid into a pulsed fluid flow;

an ejection tube that includes an opening communicating with the pulsation generator;

a suction tube into which the ejection tube is movably inserted;

an upper case and a lower case that form a body for accommodating at least the fluid chamber and the pressure generator, wherein the ejection tube extends from an outlet channel of the pulsation generator and the suction tube extends towards the body;

wherein the ejection tube is held by an inner circumferential surface of the suction tube, the suction tube has a cross sectional area in a crossing direction to an extending direction of the suction tube and the cross sectional area of the suction tube, including an inner lumen thereof, has a major axis and a minor axis; and the ejection opening is held by a portion of the suction tube corresponding to the minor axis, the portion of the

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suction tube corresponding to the minor axis comprising a substantially flat, elliptical shape, the suction tube transitioning along its length, from a tip of the suction tube towards the body, from the substantially flat, elliptical shape to another cross-sectional configuration.

2. The medical instrument according to claim 1, wherein the suction opening has a cross sectional area in the crossing direction to the extending direction of a suction tube, and the cross sectional area is a substantially elliptic shape.

3. The medical instrument according to claim 1, wherein the suction tube has another cross sectional area in the crossing direction to the extending direction of the suction tube other than a suction opening, and the cross sectional area is a substantially elliptic shape.

4. The medical instrument according to claim 1, wherein the tip of the suction tube is configured to rotatably engage with the suction tube so that the suction tube is allowed to rotate around its axis.

5. The medical instrument according to claim 1, wherein the medical instrument is for ejecting a pulsed fluid and for incising a biological tissue.

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